

D2CAN: Domain-guided contrastive adversarial network for EEG-based cross-subject cognitive workload decoding

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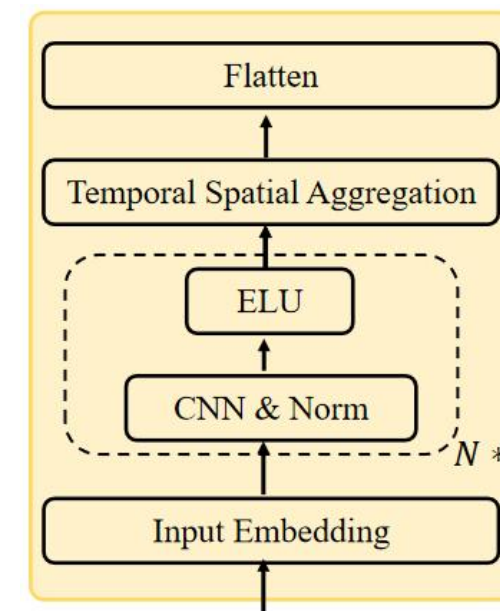
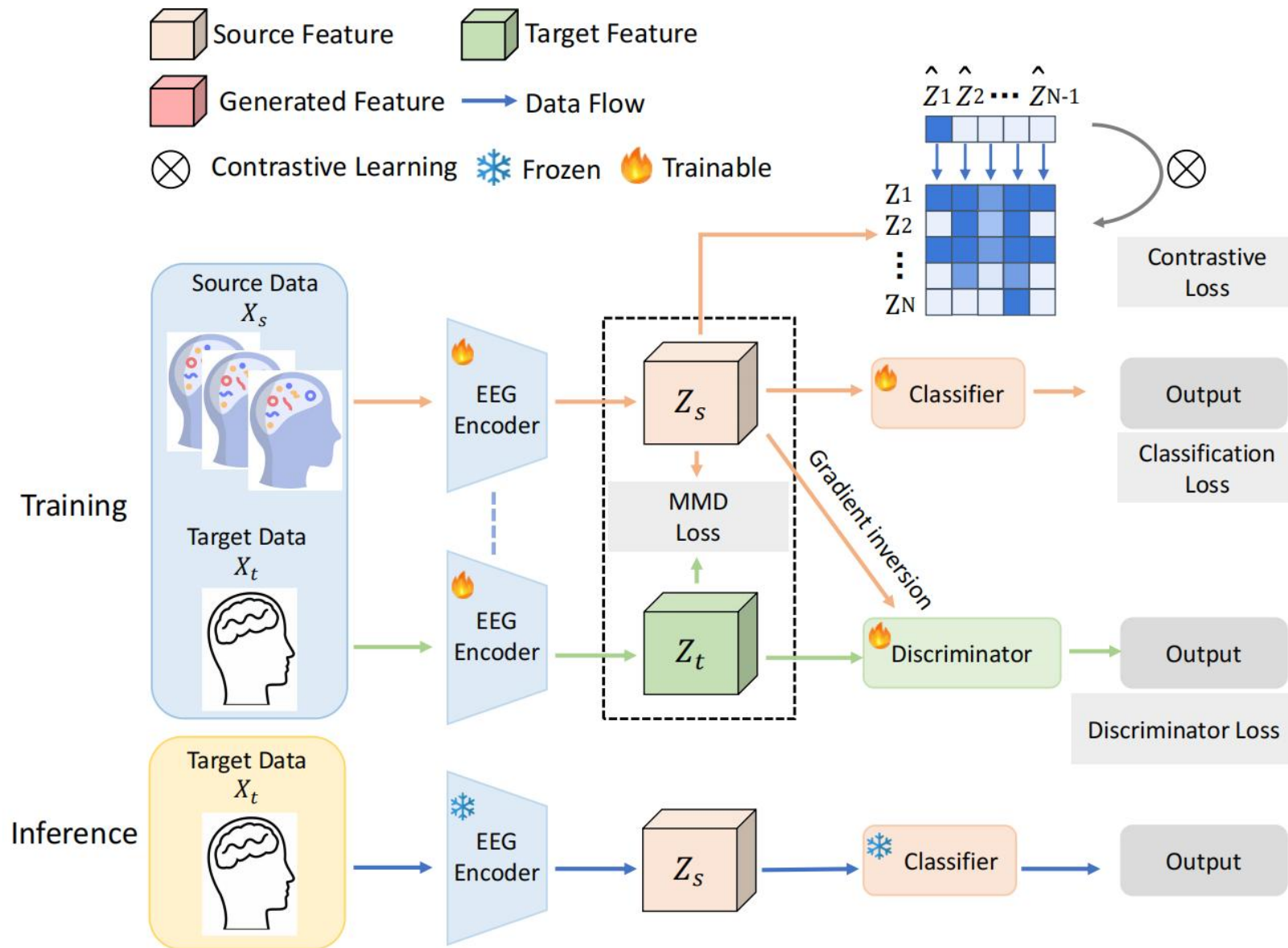
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- Cognitive workload recognition based on EEG
 - Measurement information processing
 - Optimal interaction design
 - Reduce human error

- Neural decoding based on transfer learning
 - Reduce distribution shift
 - Dealing with individual differences
 - Reduce calibration time

- Cross-subject difference
 - Individual difference
 - Non-stationarity of EEG signal
 - Label inconsistency
- Sensitive to noise
 - Low signal-to-noise ratio of EEG signals
 - Data preprocessing challenge
 - Limitations of real-time applications
- Generalization ability
 - Few samples
 - Task variance

Proposed Framework



An example of EEG Encoder

- We calculate the Maximum Mean Discrepancy (**MMD**) of the source domain features and the target domain features:

$$\mathcal{L}_{\text{mmd}} = \left\| \frac{1}{N_s} \sum_{i=1}^{N_s} \phi(X_i) - \frac{1}{N_t} \sum_{j=1}^{N_t} \phi(X_j) \right\|^2$$

Here, we use Radial Basis Function (RBF) as the kernel.

- We calculate the contrastive loss of different samples from one batch:

$$\mathcal{L}_{\text{contrast}}(\theta) = -\frac{1}{B} \sum_{i=1}^B \log \frac{\exp(s(\hat{z}_i, z_i))}{\sum_{j=1}^B \exp(s(\hat{z}_i, z_j))}$$

- Classifier:

$$\mathcal{L}_{\text{cls}} = -\sum_{c=1}^C y_c \log y_c^{\text{predict}}$$

- Discriminator:

$$\mathcal{L}_{\text{dis}} = -\sum_{j=0}^J d_j \log d_j^{\text{predict}}$$

- Total objective:

$$\mathcal{L}_{\text{total}}(\theta) = \alpha \mathcal{L}_{\text{cls}} + \theta \mathcal{L}_{\text{mmd}} + \lambda \mathcal{L}_{\text{contrastive}} + \gamma \mathcal{L}_{\text{dis}}$$

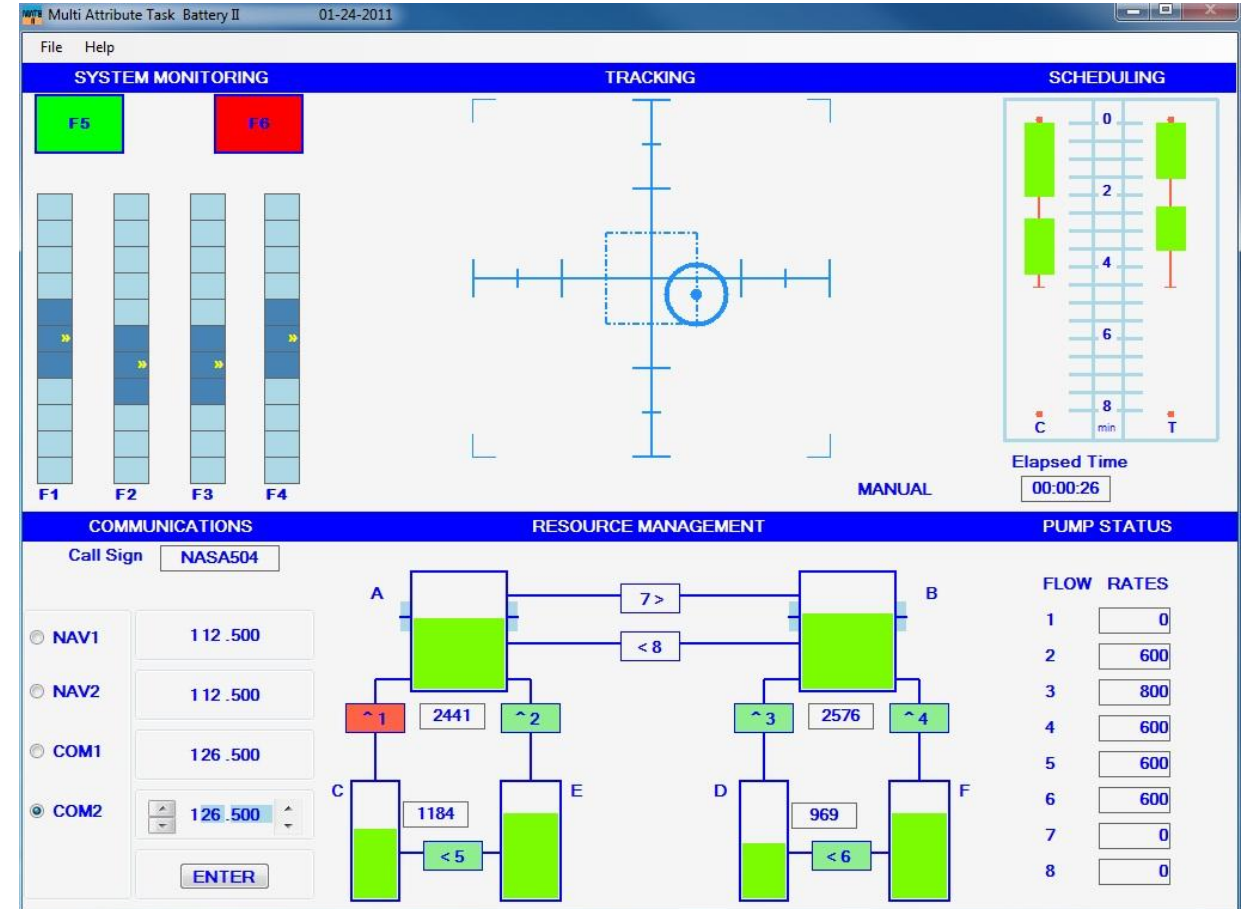
Experiments

- Datasets
 - NASA's Multi-Attribute Task Battery (MATB) task

Public dataset “Passive BCI-Hackathon Neuroergonomics conference 2021”.

- Evaluation Metrics

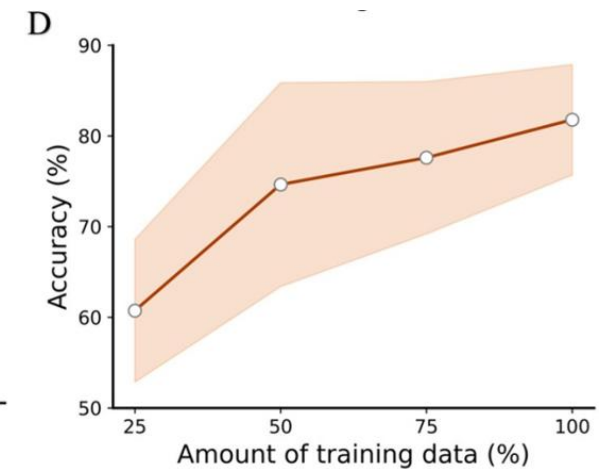
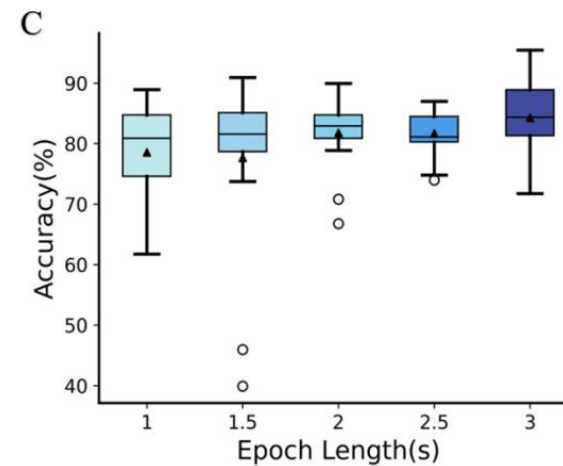
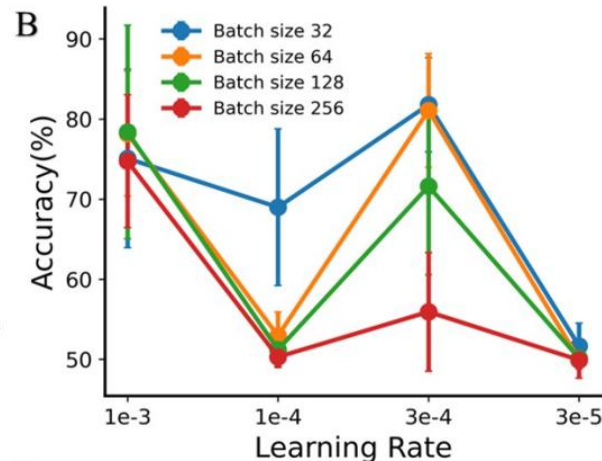
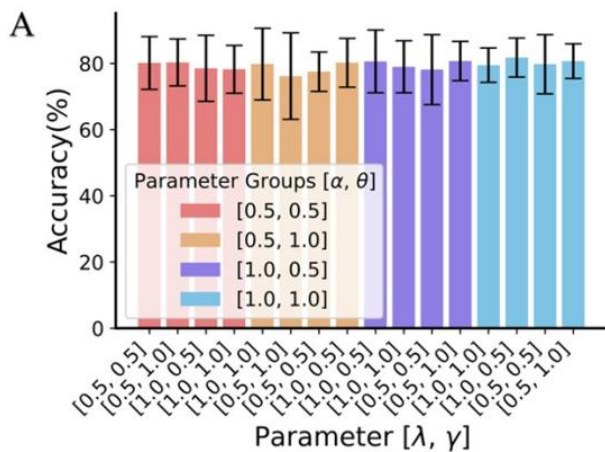
- Accuracy
- Sensitivity
- F1 Score
- Specificity
- Matthews Correlation Coefficient (MCC)



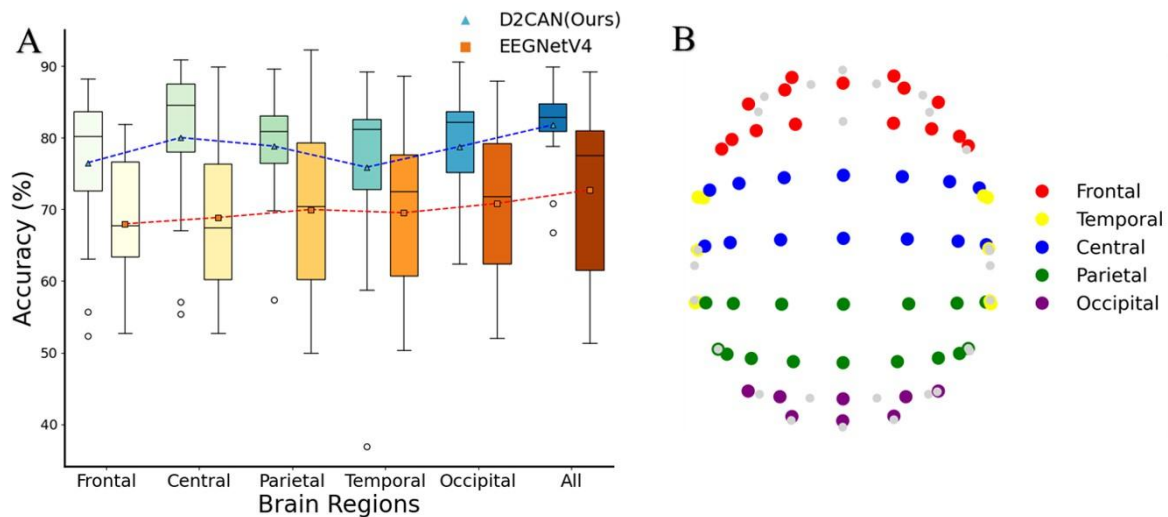
- The comparison of different baselines.:

Model	Accuracy (%)	Sensitivity (%)	F1 Score (%)	Specificity (%)	MCC (%)
SVM	67.90 ± 7.34	81.83 ± 12.17	71.72 ± 6.07	53.96 ± 17.89	38.58 ± 13.18
LDA	70.07 ± 7.78	76.33 ± 14.22	71.73 ± 6.27	63.80 ± 23.04	42.76 ± 14.82
KNN	65.75 ± 4.70	80.13 ± 9.15	69.97 ± 4.03	51.36 ± 12.76	33.58 ± 8.69
EEGNetV4	72.21 ± 12.13	74.41 ± 26.80	69.91 ± 21.01	69.75 ± 25.08	47.82 ± 20.55
ShllowCNN	71.99 ± 11.84	78.70 ± 23.26	72.42 ± 16.23	65.28 ± 31.36	48.14 ± 21.88
EEGConformer	71.57 ± 12.76	78.43 ± 24.23	72.18 ± 15.93	64.70 ± 34.82	48.00 ± 23.41
DANN	62.77 ± 9.71	62.37 ± 28.38	58.35 ± 22.87	63.18 ± 22.34	27.67 ± 19.39
DDA	73.47 ± 6.91	73.47 ± 7.15	73.11 ± 7.34	82.51 ± 7.88	48.02 ± 14.11
D2CAN (Ours)	81.79 ± 5.89	87.02 ± 8.11	82.75 ± 5.34	76.55 ± 11.63	64.68 ± 12.15

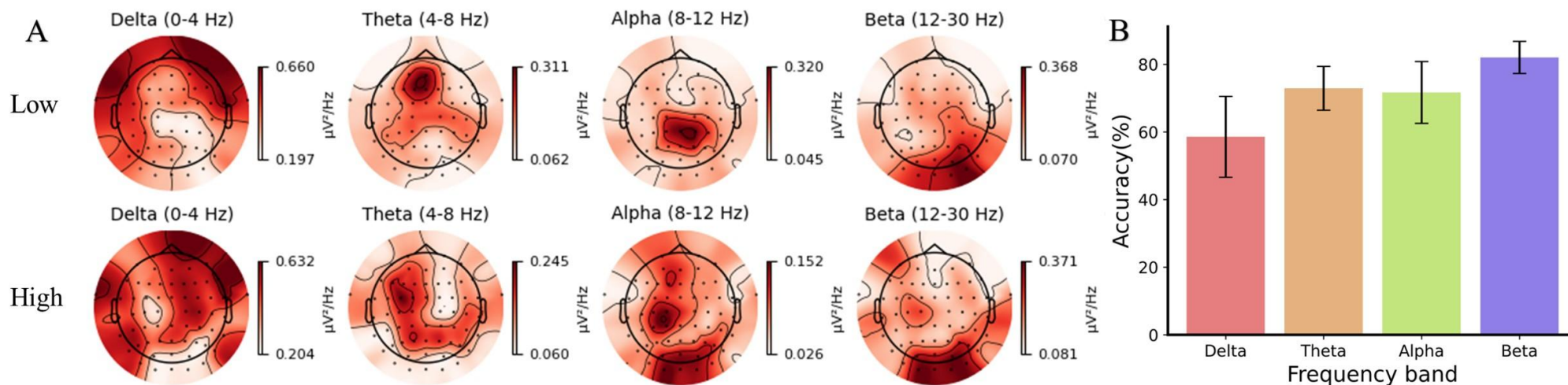
- Impact of Hyperparameters:



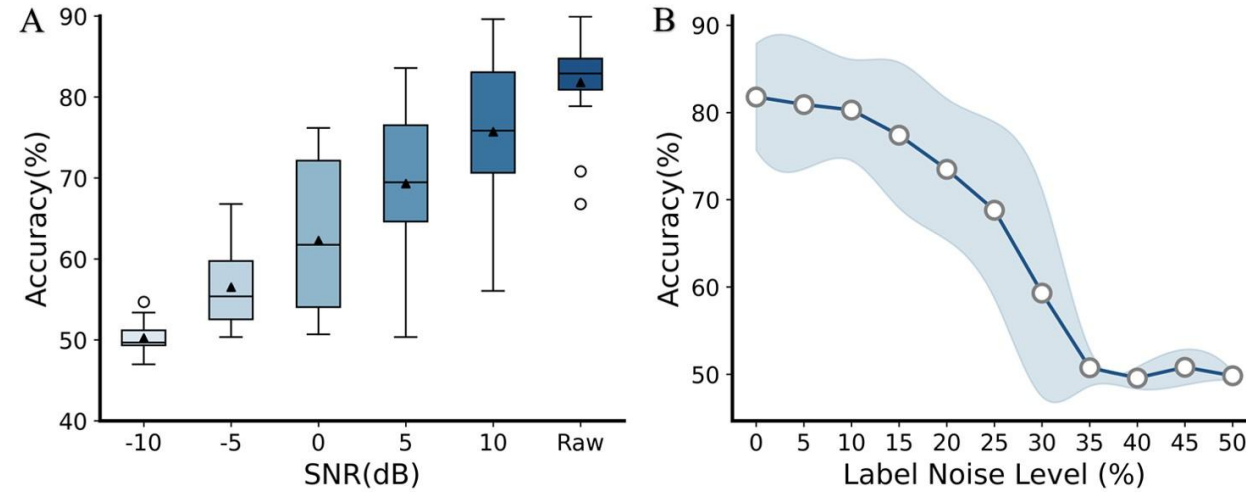
- Analysis of different brain regions (remove electrodes):



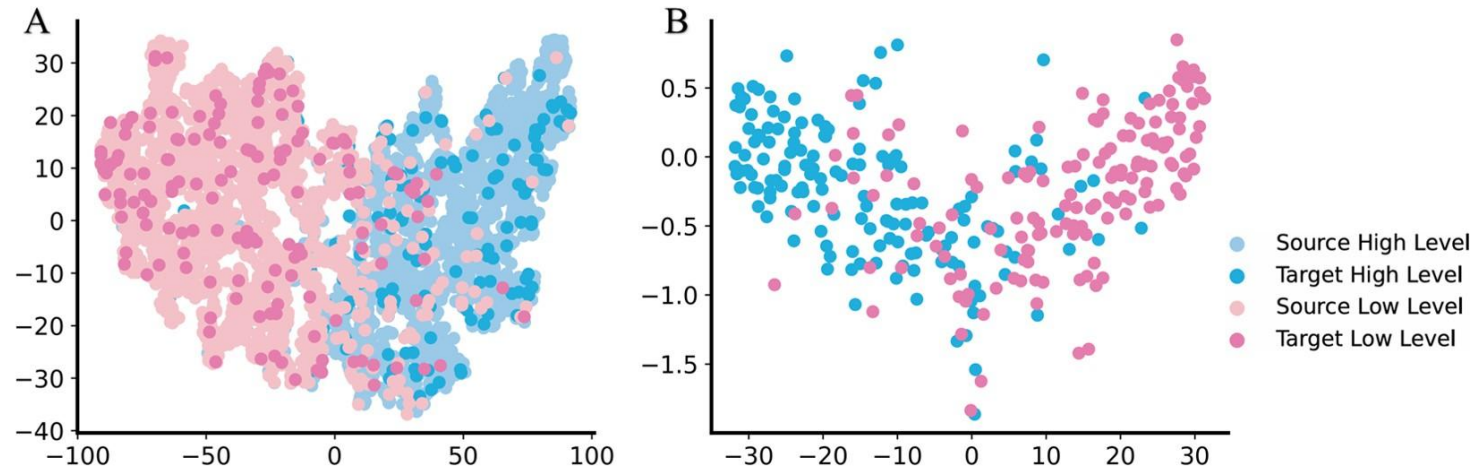
- Analysis of frequency bands:



- Noise robust analysis:



- Representative analysis:



Main Contributions:

- We propose D2CAN, a cross-subject learning framework that quickly adapts to new subjects and achieves **state-of-the-art** performance in cognitive workload decoding.
- We combine adversarial learning and **contrastive learning** to improve domain generalization for practical EEG-based cognitive workload decoding.
- We conduct extensive experiments to explore the **biological interpretability** and **robustness** of EEG-based cognitive workload decoding.

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Thanks!